

# Can red blood cell function assays assess response to red cell-modifying therapies?

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## Abstract.

**BACKGROUND:** Red blood cell (RBC)-modifying therapies have provided new opportunities for patients with sickle cell disease, although the absence of validated biomarkers of RBC function is a barrier to FDA approval and clinical adoption. Flow Adhesion (FA) and Mechanical Fragility (MF) biomarkers objectively stratify individuals with SCD into pro-adhesive vs pro-hemolytic phenotypes respectively, which may potentially help predict therapeutic responses.

**OBJECTIVE:** A Phase 3 clinical trial to determine the effectiveness of vepoloxamer, an RBC-modifying therapy in sickle cell disease (SCD), failed to meet its primary clinical outcome. The aim of this study was to determine whether standardized flow adhesion and mechanical fragility bioassays could differentiate cellular level “responders” from “non-responders” to vepoloxamer treatment.

**METHODS:** Standardized biomarkers of RBC function (adhesion and mechanical fragility) were utilized in this study to assess the effect of vepoloxamer on blood samples collected from SCD subjects and to determine whether our assays could differentiate cellular-level “responders” from “non-responders” to vepoloxamer treatment. A Wilcoxon signed-rank test was used to test for differences in adhesion in response to varying vepoloxamer treatments and a Wilcoxon Mann-Whitney test was used to assess differences in mechanical fragility, pre- and post-vepoloxamer treatment. A  $p$ -value<0.05 was considered significant.

**RESULTS:** In this study, we report that *in vitro* treatment with vepoloxamer reduced adhesion by >75% in 54% of patient samples and induced changes in the membranes of sickle erythrocytes (SSRBCs) making sickle cells behave more like normal erythrocytes (AARBCs) in terms of their resistance to hemolysis.

**CONCLUSION:** This study demonstrates that the standardized flow adhesion and mechanical fragility biomarkers described here may be useful tools to predict clinical responders to RBC-modifying therapies.

Keywords: Sickle cell disease, adhesion, vepoloxamer, mechanical fragility, blood function assays

## 1. Background

Vaso-occlusion is the primary pathophysiologic sequela of sickle cell disease (SCD), and results in intense pain and tissue damage. The accumulative life-time burden of tissue damage results in frequent, painful acute vaso-occlusive episodes (VOEs). Pain is highly subjective and a very difficult

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35 clinical outcome to measure in clinical trials and clinical practice. Other endpoints have been used  
36 such as length of stay, time to readiness for discharge, and intravenous pain medication requirements.  
37 These pain surrogates require a subjective third-party assessment and vary from patient-to-patient, thus  
38 making them inadequate clinical endpoints to assess the efficacy of an RBC-modifying therapy.

39 Sickle erythrocytes (SSRBCs) contribute to the pathogenesis of vaso-occlusion, in part, by abnor-  
40 mally adhering to the vascular endothelium. The degree of adherence correlates with clinical  
41 vaso-occlusive severity [1, 2]. Very late antigen-4 (VLA-4) is one of the most well-characterized adhe-  
42 sion receptors on SSRBCs. Reticulocyte VLA-4 expression is higher in SCD subjects with frequent  
43 VOEs and decreased in SCD patients treated with HU [3, 4]. VLA-4 is present on SSRBC popula-  
44 tions with increased adhesiveness and supports adhesion between SSRBC and endothelial vascular cell  
45 adhesion molecule-1 (VCAM-1) [5, 6]. VLA-4 on SSRBCs also mediates SSRBC and mononuclear  
46 leukocyte cell-to-cell adhesion either directly or indirectly via fibronectin, forming cell aggregates  
47 on the endothelial surface or in suspension [7, 8]. In murine SCD models, adhesion of SSRBCs and  
48 leukocytes to endothelium are reversed by antibodies that block VCAM-1 [6, 9].

49 SSRBC membrane properties play a key role in adhesive and obstructive events in SCD [10,  
50 11]. Sickle hemoglobin (HbS) polymerization critically impacts membrane structural proteins, like  
51 Band-3 complex, resulting in membrane micro-vesiculation [12]. Associated oxidative damage causes  
52 defects in membrane structures resulting in irreversible micro-rheologic abnormalities of SSRBC mem-  
53 branes,[13] structural membrane rearrangements, and ultimately plastic membrane damage [14, 15].  
54 Accumulated “sub-lethal” red blood cell (RBC) damage may be a key factor in accelerated SSRBC  
55 senescence [16] and ultimately hemolysis and/or premature cell removal from the circulation by the  
56 spleen [17]. SSRBCs with “fragile” membranes are prone to hemolysis, which results in the release  
57 of intracellular contents that promote inflammation and induce expression of adhesion molecules  
58 (e.g.VCAM-1) [18]. Destabilization of the RBC membrane and cell sickling also results in prema-  
59 ture cell destruction and release of hemoglobin, which contribute to SCD pathology by limiting nitric  
60 oxide bioavailability [19] and promoting oxidative damage [20]. Hemolysis is associated with SCD  
61 complications such as pulmonary hypertension, priapism, ulcers and stroke, [21] with even low lev-  
62 els of serum Hb increasing RBC aggregation [22]. Toxicity of cell-free Hb contributes to impaired  
63 microcirculation, vasoconstriction, diminished oxygen delivery, [23–25] as well as, proinflammatory  
64 and vaso-occlusive effects [26–28].

65 A Phase 3 clinical trial (EPIC) to determine the effectiveness of vepoloxamer (purified MST-188) in  
66 alleviating VOEs in SCD recently failed. Vepoloxamer, an amphipathic triblock copolymer, is believed  
67 to improve rheology in SCD by non-specific intercalation with the RBC membrane, resealing damaged  
68 pores and increasing lipid packing density [29, 30]. Prior clinical studies demonstrated the ability of  
69 MST-188 to reduce acute VOE duration and total opioid analgesic requirements in SCD [31]. In the  
70 EPIC trial, vepoloxamer failed to meet its primary outcome to significantly reduce the duration of acute  
71 VOEs, an endpoint based on patient’s subjective perception of pain. In the absence of standardized  
72 biomarkers of RBC function, the discrepancy between promising preclinical data and the clinical  
73 endpoints is difficult to ascertain.

74 Since the EPIC trial, there have been more promising RBC-modifying therapies that have failed  
75 to show a reduction in acute pain crises duration in phase 3 clinical trials. As more RBC modifying  
76 therapies are investigated in SCD, it is critical to deploy objective measures of cellular-level response  
77 as predictive, monitoring, and surrogate biomarkers. The aim of this study was to determine whether  
78 standardized flow adhesion and mechanical fragility bioassays could be applied to assess changes in  
79 select functional properties of RBCs induced by vepoloxamer. Simultaneous use of both Flow Adhesion  
80 (FA) and Mechanical Fragility (MF) biomarkers dovetails with the two main SCD phenotypes, adhesive  
81 and hemolytic, which can be linked to different clinical disease states, and potentially to different  
82 response to the therapy [32]. Of particular interest was whether the bioassays could differentiate

83 “responders” from “non-responders” to vepoloxamer treatment, exploring a potential scaffold for  
 84 validating biomarkers to predict clinical responders to RBC-modifying therapies.

## 85 2. Material and methods

### 86 2.1. Reagents

87 Vepoloxamer was a gift from Mast Therapeutics (San Diego, CA). Recombinant human VCAM—1  
 88 (rhVCAM-1) was purchased from R&D Systems (Minneapolis, MN) and human umbilical vein  
 89 endothelial cells (HUVECs) from Lonza (Walkersville, MD).

### 90 2.2. Blood donors

91 Informed consent protocols were performed following institutional review board (IRB) approval  
 92 by Wayne State University and the University of Michigan. Blood samples were collected in sodium  
 93 citrate from non-SCD ( $n = 15$ ) and SCD subjects (HbSS;  $n = 26$ ; Table 1).

Table 1  
SCD Demographics

Subject (#)	Age (years)	Gender	Adhesion to VCAM-1 (cells/mm <sup>2</sup> )	Adhesion to HUVECs (cells/mm <sup>2</sup> )	WBC (K/CUMM)	Hemoglobin (g/dL)	Hematocrit (%)	Platelets (K/CUMM)	Reticulocyte (%)
001	10	M	102	21	4.6	11.4	33.1	364	4.2
002	5	F	370		8.6	9	27.2	171	6.1
003	3	F	97	33	11.2	11.6	34.6	385	0.9
004	10	M	50		9.3	9.5	28.9	596	3.7
005	10	M	382	29	14.1	8.3	23.5	545	24.6
006	19	F	465		11.3	8.6	24.8	470	20.2
007	10	F	235		13.3	8.2	25	500	14
008	6	M	540		12.9	7.4	20.8	414	16.4
009	10	M	274		6.6	10.1	28.3	163	4
010	3	F	308		7.6	12.6	37.9	380	1.9
011	15	M	337		9.7	9.8	27.7	800	10.6
012	2	F	292	15	7.5	8.5	24.5	228	6.5
013	6	M	193		10.7	8.2	23.6	511	7.9
014	3	F	220		10.3	7.8	22.1	337	14.3
015	19	F	492		10.8	8	23.5	571	20.1
016	5	M	375	18	16.4	7.7	24.1	463	8.7
017	8	F	85		15.3	8.8	25.7	426	8.7
018	10	M	310		13.4	6.2	17.4	481	23.2
019	16	M	160	20	9.4	7.6	21.8	403	18.6
020	3	M	453	34	16.8	7.9	22.3	472	12.8
021	1	F	228		9.6	8.6	25.7	293	9.5
022	4	F	227		12.2	10.3	30.8	192	7.2
023	4	F	243		15.3	8.6	23.9	437	10.9
024	3	F	355	8	9.7	8.8	25.6	492	8.5
025	16	M	542	8	12.6	10.3	30.8	323	9.7
026	10	F	528						

### 2.3. Microfluidic flow-based adhesion bioassay

Flow adhesion assays were performed with a commercial well-plate, microfluidic flow system (BioFlux 1000Z, Fluxion, San Francisco, CA) by modification of published methods [33, 34]. To assess adhesion, channels were seeded with human umbilical vein endothelial cells (HUVECs; Lonza, Basel Switzerland) or coated with VCAM-1. Blood samples were pretreated with varying concentrations of vepoloxamer (0.1, 1, 10 mg/mL) and perfused through microfluidic channels during flow (1.0 dyne/cm<sup>2</sup>, 1.67 Hz). Images were acquired with a high-resolution CCD camera and analyzed with Montage imaging software (Molecular Devices, Downingtown, PA). Adherent cells were quantified to generate an adhesion index (AI; cells/mm<sup>2</sup>).

### 2.4. Mechanical fragility (MF) assay

Whole blood samples were diluted to Hb concentration of 1.7 g/dl and verified with a Hemoglobin 201 system (HemoCue; Angelholm, Sweden). Mechanical stress was applied using a TissueLyser LT (Qiagen, Dusseldorf, Germany) vertical bead mill at an oscillation frequency of 50 Hz in the presence of one 7 mm diameter stainless steel ball, as previously described [35]. Following centrifugation, hemolysis was measured in supernatants by calculating the difference between absorbance at 576 nm (wavelength of oxygenated Hb maximum) and 685 nm (local minimum for the oxygenated Hb form) using a NanoDrop N100 spectrophotometer (Thermo Scientific, Waltham, MA) while accounting for the Sowemimo-Coker correction [36]. Hemolysis metrics (Hem) were used to represent amount of hemolysis from i) a labile RBC subpopulation lysed after 3 minutes of stress application (L-Hem), ii) a more stress-resistant RBC fraction that lysed between 3 and 10 minutes of stress application (R-Hem), or iii) the cumulative hemolysis induced over the full 10 minute stress-supplication time (C-Hem). Values were obtained from best-fit second-order polynomial regression of the experimental data.

### 2.5. Statistical analysis

Statistical analysis was performed with GraphPad Prism software (San Diego, CA). Differences within each patient were analyzed using Wilcoxon signed-rank test, a non-parametric statistical hypothesis test used for repeated measurements on the same sample to compare their population means. Wilcoxon Mann-Whitney tests were used to assess differences in samples pre- and post-vepoloxamer treatment. A *p*-value <0.05 was considered significant.

## 3. Results

This study enrolled SCD volunteers (*n*=26) aged between 1 and 19 years. The study included comparable numbers of males and females and volunteers on (*N*=5) and off (*N*=21) hydroxyurea therapy. Hematology and chemistry labs were obtained during research draws. Blood samples were obtained from SCD subjects at steady state benign clinic visits.

### 3.1. Flow adhesion

Blood samples from SCD subjects were pretreated with varying concentrations of vepoloxamer (0, 0.1, 1, 10 mg/mL) and perfused through microfluidic channels seeded with HUVECs or coated with VCAM-1 to assess the effect of vepoloxamer on whole blood adhesion to HUVECS and VCAM-1. Flow conditions (1.0 dynes/cm<sup>2</sup>, 1.67 Hz) simulate blood flow in the post-capillary blood venules where these

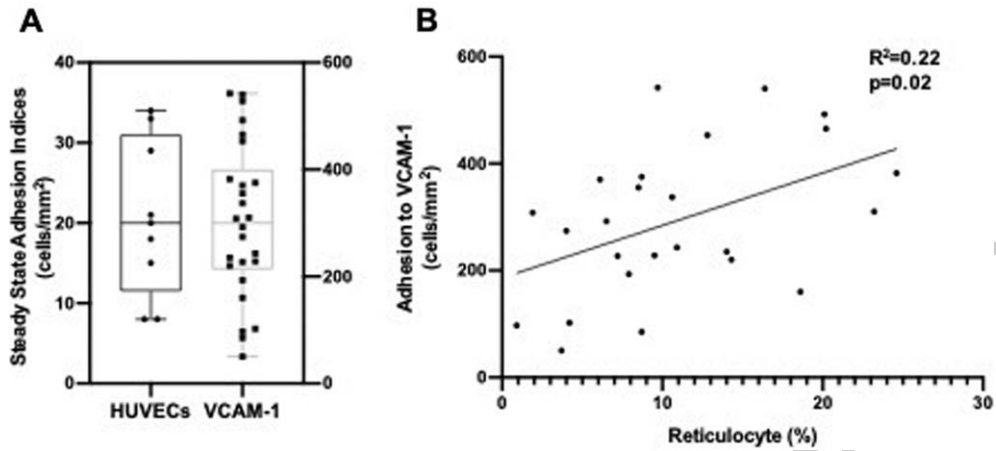


Fig. 1. Flow adhesion in SCD blood samples. A) Steady state adhesion to HUVECs (left y-axis) and VCAM-1 (right y-axis) varies in SCD blood samples. B) SSRBC adhesion to VCAM-1 correlates with reticulocyte percent.

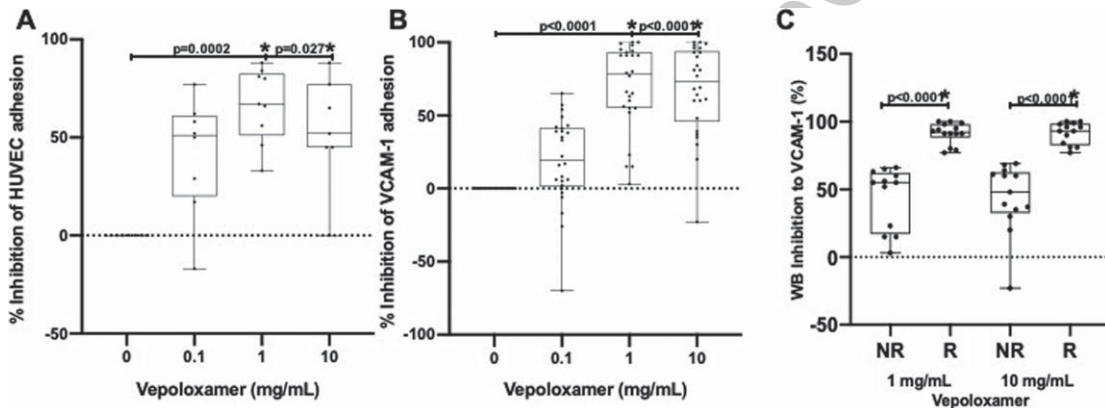


Fig. 2. Effect of vepoloxamer on SSRBC adhesion in SCD. Vepoloxamer significantly reduces adhesion to HUVECs (A) and VCAM-1 (B) in SCD blood samples. C) Vepoloxamer responders were classified as SCD patients demonstrating  $\geq 75\%$  inhibition at 1 and 10mg/mL vepoloxamer. Responder and non-responder groups were significantly different at both vepoloxamer concentrations.

132 adhesive interactions are likely to occur. Steady state adhesion varied from patient-to-patient (HUVECs:  
 133 mean =  $20.67 \pm 28.4$  cells/mm<sup>2</sup>, range = 8–34 cells/mm<sup>2</sup>; VCAM-1: mean =  $302.4 \pm 3.2$  cells/mm<sup>2</sup>,  
 134 range = 50–492 cells/mm<sup>2</sup>; Fig. 1A). As shown in prior studies [33], steady state adhesion of whole  
 135 blood to VCAM-1 was significantly higher in SCD subjects with higher reticulocyte counts ( $R^2 = 0.22$ ;  
 136  $p = 0.017$ ; Fig. 1B), although steady state adhesion of whole blood to HUVECs did not correlate  
 137 with clinical lab data (data not shown). Vepoloxamer (0.1, 1, and 10 mg/mL) significantly reduced  
 138 adhesion to HUVECs (mean = 41% inhibition,  $p = 0.0002$ ; Fig. 2A) and VCAM-1 (mean = 69.5%  
 139 inhibition,  $p < 0.0001$ ; Fig. 2B) at 1 mg/mL. Steady state adhesion indices were not predictive of  
 140 cellular-level response to vepoloxamer (data not shown). 54% of patients' samples were classified as  
 141 responders ( $n = 14$ ; from 44.0 to 91.4%) at 1 and 10 mg/mL vepoloxamer, while 46% were classified  
 as non-responders ( $n = 12$ ; from 43.7 to 91.4%) (Fig. 2C).

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### 3.2. Mechanical fragility

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Mechanical fragility was assessed at baseline and at 1 mg/mL vepoloxamer. The higher volume requirement for this assay precluded testing multiple doses. A statistically significant reduction in L-Hem ( $p = 0.0452$ ) was observed in response to 1 mg/mL vepoloxamer treatment of SSRBCs, whereas there was no significant difference observed in the more resistant fraction, R-Hem ( $p = 0.6162$ ) and C-Hem ( $p = 0.0892$ ) (Fig. 3A; Table 2).

In untreated SSRBC blood samples, induced hemolysis in both labile (L-Hem;  $p = 0.0003$ ) and cumulative (C-Hem;  $p = 0.0147$ ) SSRBC fractions was significantly elevated as compared to normal

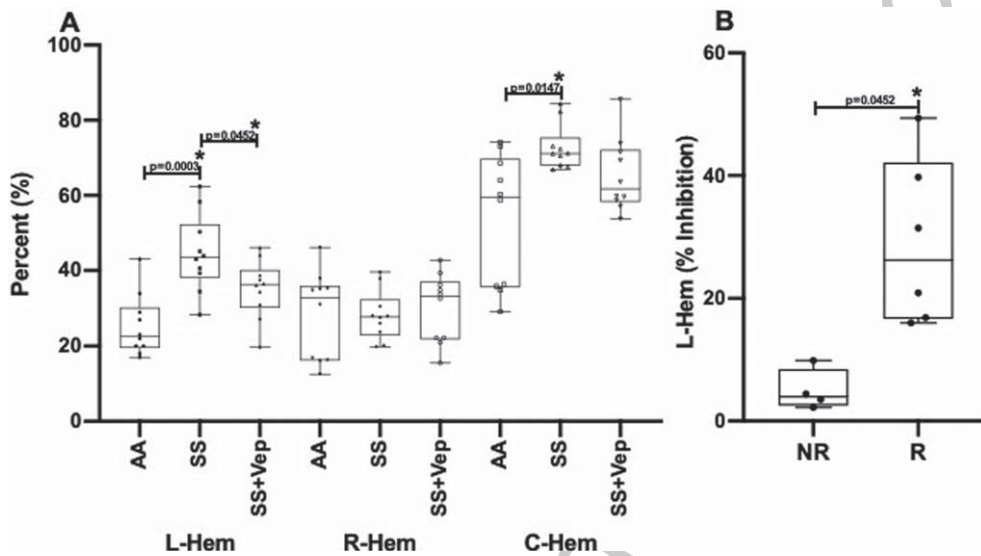


Fig. 3. Vepoloxamer reduces mechanical fragility in SSRBCs. A) Induced hemolysis in labile (L-Hem;  $p = 0.0003$ ) and cumulative (C-Hem;  $p = 0.0147$ ) SSRBC fractions was significantly higher than normal erythrocytes (AARBCs), however there was no difference for the resistant fraction (R-Hem). Vepoloxamer (1 mg/mL) significantly reduced L-Hem ( $p = 0.0452$ ), whereas there was no significant difference observed in the more resistant fraction, R-Hem ( $p = 0.6162$ ), and C-Hem ( $p = 0.0892$ ). B) SCD subjects were stratified into two groups based on the magnitude of the decline in labile SSRBC fractions (L-Hem) in the presence of vepoloxamer and designated as “responder” or “non-responders”.

Table 2  
Mechanical Fragility

Subject (#)	Normal (AA)			SCD (Untreated)			SCD (1mg/mL Vepoloxamer)		
	L-Hem	R-Hem	C-Hem	L-Hem	R-Hem	C-Hem	L-Hem	R-Hem	C-Hem
001	23.49	35.27	58.76	28.4	39.6	68	27.4	36.2	63.6
002	22.50	37.75	60.25	45.1	28	73.1	44.1	15.5	59.6
003	29.16	34.82	63.99	40.6	30.6	71.2	38.8	32.7	71.5
004	18.06	16.80	34.86	34.5	37.9	72.4	31.1	42.8	73.9
005	26.94	46.07	73.01	43	28.1	71.1	36.1	21	57.1
006	20.08	16.26	36.34	43.9	23.8	67.7	36.5	22.2	58.7
007	19.87	16.05	35.91	58.3	26.1	84.4	46.1	39.4	85.5
008	16.62	12.55	29.17	50.3	20.2	70.5	34.5	34.9	69.4
009	43.04	31.05	74.09	39.3	27.6	66.9	19.9	33.9	53.8
010	33.55	35.09	68.64	62.4	19.9	82.3	37.6	22.2	59.8

erythrocytes (AARBCs), however significance was not achieved for the more resistant fraction (R-Hem;  $p > 0.9999$ ) (Fig. 3A; Table 2). Similar to the difference between SSRBCs and AARBCs, following vepoloxamer treatment of SSRBCs, C-HEM was no longer significant ( $p = 0.00892$ ).

SSRBC exhibited significant subject-to-subject variability in the magnitude of vepoloxamer-associated reduction in induced hemolysis. SCD subjects in this study can be stratified into two groups based on the magnitude of the decline in labile SSRBC fractions (L-HEM) in the presence of vepoloxamer. The average decline in L-Hem on vepoloxamer supplementation was  $19.44 \pm 5.097$  percent with subjects naturally falling into two groups based on their response to therapy (Fig. 3B). The “responder” group showed a decline in L-HEM ( $29.06 \pm 5.527\%$ ) vs. “non-responders” ( $5.007 \pm 1.679\%$ ). This difference was statistically significant ( $p$ -value = 0.0095). While there was no statistically significant difference between the two groups in white blood cell count, total hemoglobin, hematocrit or platelet count, the groups demonstrated significant difference in reticulocyte counts (responders:  $7 \pm 4$ , non-responders:  $15 \pm 5\%$ ;  $p < 0.05$ ).

#### 4. Discussion

Standardized biomarkers of RBC function (adhesion and mechanical fragility) were utilized in this study to assess the effect of vepoloxamer on blood samples collected from SCD subjects and to determine whether our assays could differentiate cellular-level “responders” from “non-responders” to vepoloxamer treatment. Adhesion indices, obtained from our standardized, flow-based adhesion bioassay, varied from patient-to-patient in SCD subjects at steady state and likely represents highly variable SCD phenotypes amongst patients. Adhesion indices were correlated with hematologic parameters to identify influencers of adhesion in our flow system. Steady state adhesion of whole blood to VCAM-1 positively correlated with reticulocyte percent. Reticulocytes highly express VLA-4, a ligand for VCAM-1, which likely accounts for the positive relationship with adhesion to VCAM-1.

Blood samples pretreated with vepoloxamer (0.1, 1, and 10 mg/mL) significantly reduced adhesion to HUVECs and VCAM-1 at 1 mg/mL. Similarly, previous reports have demonstrated that vepoloxamer reduces adhesion to microvascular endothelial cells [37]. HUVECs, a macro-vascular cell line, has been used in numerous sickle cell, flow-adhesion studies to evaluate SSRBC adhesion to an endothelial substrate [6, 38, 39]. TNF-alpha upregulates the expression of VCAM-1 on the endothelial surface [40]. While stimulated HUVECs used in this study are an effective *in vitro* model, integration of an endothelial cell-based bioassay into clinical studies is not practical. VCAM-1 is a more reliable, standardized alternative for assessing RBC adhesive properties. Interestingly, vepoloxamer’s non-specific mechanism did not interfere with its ability to inhibit specific high avidity interactions such as VLA-4/VCAM-1. These data validate the use of an isolated adhesive substrate as a surrogate for a more physiologic endothelial substrate in a standardized clinical adhesion assay.

The *in vitro* effect of vepoloxamer was highly variable in this sickle cell population, similar to the variable response observed in prior studies evaluating blood function biomarkers [41, 42] and clinical response to SCD-modifying therapy given in the acute setting [43], as well as, maintenance therapy [44, 45]. Steady state adhesion indices were not predictive of cellular-level response to vepoloxamer. *In vitro* treatment with vepoloxamer reduced adhesion by  $> 75\%$  in 54% of patient samples may be useful tools to predict clinical responders to RBC-modifying therapies.

For the purposes of this study, we set 75% inhibition as the “responder” threshold. Based on this definition 54% of patients’ samples were classified as responders at 1 and 10 mg/mL doses of vepoloxamer concentrations, while 46% were classified as non-responders.

Elevated mechanical fragility in SSRBCs, as compared to AARBCs, has been reported previously [14, 46] along with high subject-to-subject variability, however those studies did not differentiate

195 between RBC fractions based on their stability under applied stress. The findings presented here  
196 indicate that vepoloxamer induced changes in the membranes of SSRBCs making sickle cells behave  
197 more like AARBCs in terms of their resistance to hemolysis. This “normalization” of sickle cell  
198 response to stress relative to cells from normal donors, can be interpreted in terms of the compound  
199 facilitating stabilization of RBC membranes through the reversal of accumulated polymerization-  
200 induced membrane damage. Mechanical Fragility data indicate that vepoloxamer predominantly affects  
201 labile/fragile (less resistant to mechanical stress) SSRBC fractions (described by L-Hem). The labile  
202 fraction of RBCs is characterized by higher accumulated sub-hemolytic membrane damage. Our data is  
203 consistent with vepoloxamer’s mechanism of action which is expected to have little or no effect on cells  
204 with less perturbed membranes that are presumably less susceptible to hemolysis. These findings also  
205 align with previous reports demonstrating that vepoloxamer reduced hemolysis during RBC storage  
206 and increases preservation of the most labile cell fraction (impact on more resistant cell fractions was  
207 not assessed) [47].

208 These observations are consistent with the observation that the responder group had elevated, retic-  
209 ulocyte counts compared to non-responders. High reticulocyte counts reflect a potentially younger  
210 average sickle RBC populations, presumably with less accumulated membrane damage due to cell  
211 age and thus to potentially fewer incidences of polymerization-inducing hypoxia. It could be indeed  
212 expected that such RBC populations with less accumulated membrane damage would be less impacted  
213 by vepoloxamer treatment. Sandor et. al. reported that RBC deformability assessed by ektacytometry  
214 and microfluidics, was not affected by vepoloxamer [37]. These data were interpreted by the authors  
215 to suggest that vepoloxamer “does not affect RBC mechanical properties”, thus contradicting the data  
216 reported here. However, RBC deformability and MF are regulated by different interactions of skeletal  
217 proteins [48]. Although related, the effect of RBC-modifying therapies on these membrane properties  
218 are not necessarily identical. The hemolytic propensity of RBCs is known to vary significantly between  
219 individuals, [49] due in part to individual differences in RBC metabolic age [50, 51] and ATP levels,  
220 [52–54] with likely contributions from ethnicity, age, gender, lifestyle, and genetic pathologies [55–57].  
221 Subject-to-subject variability may be a root cause of differences between an individual’s response to  
222 vepoloxamer as assessed by either VCAM-1 adhesion or RBC MF. Differences in the severity of sub-  
223 hemolytic SSRBC damage and adhesive properties between patients may be further amplified by the  
224 history of hypoxic events and VOEs, and treatment, including hydroxyurea and transfusions [14].

225 While the causes of differences between responders and non-responders in our study remain to  
226 be elucidated, it can be suggested that those may be related to the amount and types of preexisting  
227 membrane perturbations and/or damage. For example, the asymmetrical distribution of phospholipids  
228 is well conserved throughout the RBC lifespan and its exposure on the membrane surface plays a key  
229 role in RBC apoptosis and removal from circulation [58, 59]. Similar to senescent RBCs, abnormal  
230 erythrocytes with e.g. membrane disorders, have PS exposed on the external membrane resulting in  
231 premature hemolysis [60]. Elevated PS exposure had been suggested as one of the key features of  
232 sickle RBC impaired survival in circulation [61] with strong positive correlation observed between  
233 exposed PS and cellular adhesion in SCD [62]. Notably, the levels of PS exposure vary significantly  
234 even between normal donors, contributing e.g. to RBC loss of viability during storage with original,  
235 pre-collection, PS expose levels correlated with RBC oxidative stress markers and fragility [57].

236 Despite progress made in understanding of molecular mechanisms behind SCD phenomena, lack of  
237 reliable biomarkers remains a major barrier to approving emerging therapies in SCD. In this study, we  
238 demonstrated that the flow adhesion assay could identify 54% of the vepoloxamer-treated population as  
239 responders (>75% inhibition of adhesion). Previous studies have established that baseline adhesion to  
240 VCAM correlates to historical disease severity [63]. As a result, vepoloxamer-induced normalization  
241 of adhesion indices in 54% of the population may correlate to a clinical response as well. Additionally,  
242 our data demonstrated that vepoloxamer predominantly affected more labile/fragile RBC populations,



likely characterized by higher accumulated sub-hemolytic membrane damage. As a result, elevated labile fraction of RBCs, as indicated by the mechanical fragility index, may identify individuals more likely to respond to RBC-modifying therapies such as vepoloxamer. Present work shows the potential of drug-induced normalization in adhesion and fragility could serve as surrogate biomarkers for RBC-modifying therapies. In addition to providing new tools for monitoring a patient's response to therapy, utilization of such biomarkers could enable efficient stratification of patients based on likelihood of therapeutic response and/or allow for enrichment in clinical trials by developing and implementing optimal inclusion/exclusion criteria.

The magnitude of clinically meaningful response to a therapy cannot be ascertained solely through pharmacodynamic response to *in vitro* treatment, but ultimately requires confirmation from biomarker data obtained from treated patients. Variability observed in vepoloxamer response utilizing our flow adhesion and mechanical fragility assays allowed for potential stratification of SCD subjects based on *in vitro* response and showed the potential of RBC functional assays to differentiate patients based on cellular level pharmacodynamic responses to a RBC-modifying therapy. However, the clinical relevance of responder vs. non-responder stratification remains yet to be validated through clinical outcomes. Further studies are ongoing to determine the utility of RBC function assays such as flow adhesion and mechanical fragility to predict and monitor therapeutic response in both clinical trials and clinical practice.

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## Authorship contributions

Jennell White: Experimental design and execution, data analysis, and manuscript preparation.

Xiufeng Gao: Data analysis, and manuscript preparation.

Michael Tarasev: Data acquisition and analysis, and manuscript preparation.

Sumita Chakraborty: Data acquisition and analysis.

Ke Liu: Data analysis, and manuscript preparation.

Marty Emanuele: Data analysis and manuscript review.

Patrick Hines: Project conception and experimental design, and manuscript preparation.

## Conflict of interest statement

J. White, X. Gao, M. Tarasev, and P. Hines are employees and shareholders of Functional Fluidics Incorporated, a company developing and commercializing assays for blood cell assessment. M. Tarasev and S. Chakraborty are shareholders of Blaze Medical Devices, a company holding some of the intellectual property pertaining to Mechanical Fragility assays. M. Emanuele was a shareholder of Mast Therapeutics, who participated in the manuscript review in his private capacity. Financial support was received from Mast Therapeutics for the completion of the study. Mast Therapeutics did not participate in the design of the study or in the interpretation of the study results and no longer pursues the use of vepoloxamer for treatment of SCD.

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